



# Aging decreases osteocyte peri-lacunar-canalicular system turnover in female C57BL/6JN mice

Ghazal Vahidi, C. Boone, F.O. Hoffman, Chelsea M. Heveran

© This manuscript version is made available under the CC-BY-NC-ND 4.0 license <https://creativecommons.org/licenses/by-nc-nd/4.0/>

**Accessibility Disclaimer:**

For a more accessible version of this document, please submit an accessibility request form through the Montana State University Library website.

1 **Aging decreases osteocyte lacunar canalicular turnover in female C57BL/6JN mice**

2

3 Ghazal Vahidi<sup>a</sup>, Connor Boone<sup>a</sup>, Fawn Hoffman<sup>b</sup>, & Chelsea Heveran<sup>a†</sup>

4 <sup>a</sup>Department of Mechanical & Industrial Engineering, Montana State University, Bozeman, MT, USA

5 <sup>b</sup>Department of Biomedical Sciences, College of Idaho, Caldwell, ID, USA

6 <sup>†</sup>Corresponding Author, T +1 406-994-2010, E [chelsea.heveran@montana.edu](mailto:chelsea.heveran@montana.edu),

7 <https://orcid.org/0000-0002-1406-7439>

8 **Abstract**

9 Osteocytes engage in bone resorption and mineralization surrounding their expansive lacunar-canalicular  
10 system (LCS) through peri-LCS turnover. However, fundamental questions persist about where, when,  
11 and how often osteocytes engage in peri-LCS turnover and how these processes change with aging.  
12 Furthermore, whether peri-LCS turnover depends on tissue strain remains unexplored. To address these  
13 questions, we utilized confocal scanning microscopy, immunohistochemistry, and scanning electron  
14 microscopy to characterize osteocyte peri-LCS turnover in the cortical (mid-diaphysis) and cancellous  
15 (metaphysis) femurs from young adult (5 mo) and early-old-age (22 mo) female C57BL/6JN mice. LCS  
16 bone mineralization was measured by the presence of perilacunar fluorochrome labels. LCS bone  
17 resorption was measured by immunohistochemical marker of bone resorption. The dynamics of peri-LCS  
18 turnover were estimated from serial fluorochrome labeling, where each mouse was administered two  
19 labels between 2 and 16 days before euthanasia. Osteocyte participation in mineralizing their  
20 surroundings is highly abundant in both cortical and cancellous bone of young adult mice but  
21 significantly decreases with aging. LCS bone resorption also decreases with aging. Aging has a greater  
22 impact on peri-LCS turnover dynamics in cancellous bone than in cortical bone. Lacunae with recent peri-  
23 LCS turnover are larger in both age groups. Our data support the hypothesis that peri-LCS turnover is  
24 associated with cortical and intracortical positions for 22 mo mice but not for 5 mo mice. The impact of  
25 aging on decreasing peri-LCS turnover may have significant implications for bone quality and  
26 mechanosensation.

27

28 **Keywords:** Aging, osteocyte, lacunar-canalicular turnover, tissue strain

29

## 30 **1.0 Introduction**

31 The loss of bone fracture resistance in aging is a major public health problem<sup>1</sup>. Osteocytes, the most  
32 abundant and longest-lived bone cells<sup>2,3</sup>, are well known to regulate both bone mass and bone matrix  
33 quality through the coordination of osteoblasts and osteoclasts<sup>2-4</sup>. The osteocyte is the topic of interest for  
34 new approaches to manage bone fragility in aging, since over time many of these cells become senescent  
35 or apoptotic<sup>5,6</sup> and require greater strains to engage anabolic signaling<sup>7-10</sup>. Osteocytes live in a porous  
36 network within lacunae connected by canaliculi and can remove and replace (i.e., turn over) bone  
37 surrounding this network<sup>2-4,11,12</sup> (**Figure 1A**). There is abundant evidence that aging decreases lacunar and  
38 canalicular sizes and connectivity in both rodents and humans<sup>11-16</sup>. These geometric changes imply that  
39 bone resorption and mineralization by osteocytes alongside the lacunar-canalicular system (LCS) also  
40 shift in aging, with possible impacts to bone quality and mechanosensation<sup>2-4,8,11,17</sup>. However, many  
41 fundamental knowledge gaps persist about how osteocytes interact with their surrounding bone tissue and  
42 how these processes change in aging.

43 The impacts of osteocyte peri-LCS turnover (alternatively termed perilacunar or lacunar-canalicular  
44 remodeling) on the aging skeleton are uncertain, in part because the percentage of osteocytes that engage  
45 in bone resorption or mineralization alongside the LCS is unknown<sup>2,3,11,12</sup>. As witnessed in studies of  
46 rodent lactation or PTH treatment, osteocytes can expand lacunae and canaliculi through production of  
47 acids as well as enzymes such as cathepsins and matrix metalloproteinases (MMPs)<sup>11,12,18-25</sup>. These pores  
48 can then recover to their original size, implying bone re-mineralization<sup>19,24</sup>. When mice are injected with  
49 fluorochrome labels after weaning, abundant fluorochrome labels are observed<sup>19</sup>. However, labeled  
50 osteocyte lacunae are also seen in several studies where rodents were not under applied calcium  
51 pressure<sup>26-28</sup>, which suggests that osteocyte LCS mineralization may be a more active and widespread  
52 phenomenon than has been previously appreciated. For example, we previously demonstrated that ~60%  
53 of randomly-selected lacunae from the femoral midshaft cross-section were labeled with calcein  
54 administered 2 days before euthanasia in 5-month and 22-month female C57BL/6 mice<sup>26</sup>. In another  
55 study, ~60% of the lacunae in the femoral midshaft cross-section of wild-type male and female C57BL/6  
56 mice at 28-day had calcein labels administered 2 days before euthanasia<sup>28</sup>. Another group found that in  
57 the mid cortical cross-section of tibia, ~55% of lacunae showed calcein labels injected 5 days before  
58 euthanasia in 2-month male wildtype littermates of MMP13 knockout mice with a mixed C57BL/6  
59 genetic background<sup>27</sup>. These studies differ in age, label dosage, time of injection, region of evaluation,  
60 and mouse genetic background. Furthermore, while cortical and cancellous bone differ in their metabolic  
61 activities<sup>29-31</sup>, it is unknown whether osteocyte peri-LCS turnover activity varies between these  
62 compartments. To investigate the potential impact of peri-LCS turnover on bone quality and

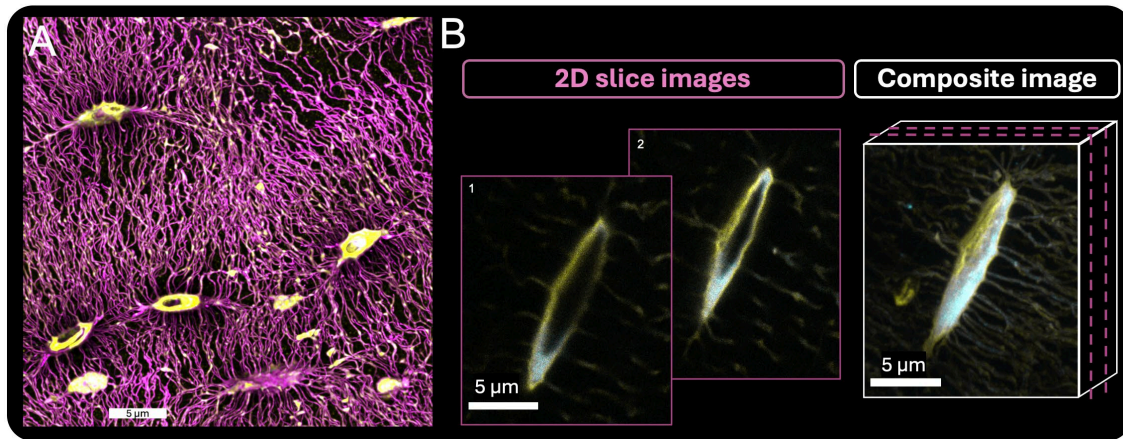
63 mechanosensation in aging, it is essential to determine the percentage of osteocytes participating in  
64 mineralization and resorption in both young adult and aged mice.

65 The dynamics of peri-LCS turnover are also essential to defining the potential impact of the  
66 osteocyte on its surrounding bone. These dynamics have been challenging to study, since LCS bone  
67 mineralization and resorption require different bone preparation and analyses. The percentage of  
68 osteocytes participating in LCS bone mineralization can be monitored by fluorochrome labeling<sup>11,12,23-28</sup>  
69 (**Figure 1**). The percentage of osteocytes resorbing bone is instead measured through  
70 immunohistochemical markers of matrix metalloproteinases and other targets<sup>13,27,28</sup> (**Figure 2D**).  
71 However, there has been a need for an approach to estimate the dynamics of bone turnover from the same  
72 bone sections. Serial fluorochrome label injections at short intervals before euthanasia can help address  
73 this gap in knowledge (**Figure 1B**). It is not possible to assess whether an individual mouse had labeled  
74 bone that was later removed. However, the average percentage of lacunae showing labels administered at  
75 specific time points (e.g., 2 through 16 days) can allow estimation of how long labels persist following  
76 deposition. Furthermore, when serial labels are delivered to the same mice, double labels can provide an  
77 indication of how long LCS mineralization can occur (**Figure 1B**). Double labels have thus far only been  
78 quantified in lactation studies as evidence of bone infilling following the removal of calcium pressure  
79 with weaning<sup>19</sup>. To interpret these peri-LCS turnover dynamics, it is also necessary to assess whether  
80 common fluorochrome labels (i.e., calcein and alizarin) show similar retention around osteocyte lacunae.

81 Another question is whether osteocyte peri-LCS turnover is mechanosensitive and if the dependence  
82 of this process on tissue strain changes with aging. Osteocytes are mechanosensitive cells and their  
83 signaling activity depends on tissue strain<sup>2,3,7,32,33</sup>. Moreover, osteocytes are less mechanosensitive in  
84 aging and require greater strains to engage anabolic signaling<sup>7-10,13</sup>. peri-LCS turnover has the potential to  
85 influence osteocyte mechanosensation through altering the shape of the porous LCS network as well as  
86 the flow characteristics within it<sup>34-37</sup>. Furthermore, as shown in our recent work using atomic force  
87 microscopy, recent LCS mineralization increases the compliance of bone within several hundred  
88 nanometers of LCS walls<sup>26</sup>, which would likely contribute towards strain amplification<sup>37</sup>. However,  
89 whether peri-LCS turnover influences - or is influenced by - strains experienced by the osteocyte is not  
90 yet understood. Since long bones experience tissue strains that vary in direction and magnitude<sup>38,39</sup>,  
91 determining how peri-LCS turnover varies throughout femoral cross-sections can help answer first  
92 questions about whether this process is associated with tissue strain in young adult and aged mice.

93 The purpose of this study is to test the hypothesis that aging decreases the percentage of osteocytes  
94 engaged in LCS bone mineralization and resorption and alters the dynamics of these processes. This  
95 hypothesis was tested by serial fluorochrome labeling and immunohistochemistry studies of cortical and  
96 cancellous bones of the femur in 5-month and 22-month female C57BL/6JN mice. We further

97 hypothesized that the peri-LCS turnover activity depends on variation in tissue strain and that this  
98 relationship changes in aging, which we tested by comparing LCS bone mineralization dynamics between  
99 femur regions of interest and with distance from the endocortical to periosteal surfaces. Moreover, we  
100 hypothesized that peri-LCS turnover activity and impacts of aging would vary for osteocytes located in  
101 the lamellar versus non-lamellar compartments of cortical bone, considering previous findings indicating  
102 that osteocyte lacunar geometry is influenced by bone structural organization<sup>40,41</sup>.



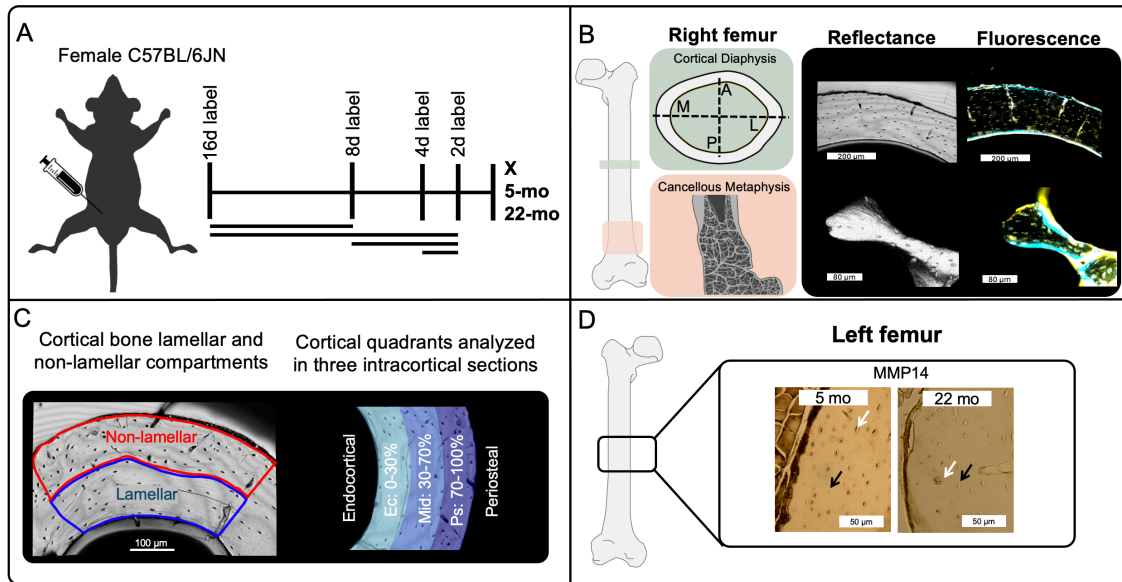
103  
104 **Figure 1.** Osteocyte lacunar-canalicular system (LCS). A) Osteocytes live in an expansive and intricate network of  
105 lacunar holes and canalicular channels. Basic fuchsin staining (magenta, *ex vivo* staining of embedded bones) shows  
106 the extensive LCS porosity of cortical bone. Calcein-stained tissue (yellow, *in vivo* fluorochrome injection 2 days  
107 before euthanasia) indicates bone mineralization. B) Osteocyte lacunae can show double labels when administered at  
108 short timepoints before euthanasia. *In vivo* serial fluorochrome labeling (calcein in yellow, 2 days before euthanasia;  
109 alizarin in blue, 8 days before euthanasia) in a female 5 mo C57BL/6JN mouse reveals double-labeled lacunae.  
110 Figure 1 generated by G. Vahidi and reprinted with permission from Current Osteoporosis Reports.

## 111 2.0 Materials and Methods

### 112 2.1 Animals

113 All animal procedures were approved by Montana State University's Institutional Animal Care and  
114 Use Committee. 5 months old young adult (5 mo, n = 20) and 22 months old early-old-age (22 mo, n=16)  
115 female C57BL/6JN mice from the National Institutes of Aging colony were utilized in this study. Mice  
116 had a minimum of two weeks to acclimatize to the MSU animal facility before the beginning of the label  
117 studies. Mice had *ad libitum* access to water and standard chow. Each mouse was administrated two  
118 intraperitoneal injections of fluorochrome labels, calcein (20 mg/kg, i.p.) and alizarin (30 mg/kg, i.p.) at  
119 two specific dates that varied for each group of mice. The goal was to collect data for injection dates that  
120 include 16d, 8d, 4d, or 2d before the euthanasia, while each group of mice received only two injections  
121 with specific timing and sequence of the injections (**Figure 2A**). For example, a group of mice received  
122 2d calcein and 4d alizarin whereas another group received 2d alizarin and 16d calcein. To ensure that  
123 label identity was not confounded with the specific time points, some mice received the calcein injection  
124 first and the alizarin injection second. Other mice received label injections in the opposite order. No

125 significant effects of label type (i.e., alizarin or calcein) were observed on the percentage of labeled  
 126 lacunae (**Figure S1**). Therefore, we aggregated the label identity data, pooling alizarin and calcein data  
 127 for each label date with  $n = 4-16$  sample per age/label date group. Labeling group sample sizes were as  
 128 followed: in 5 mo group, mice received labels at 2d ( $n=16$ ), 4d ( $n=6$ ), 8d ( $n=10$ ), or 16d ( $n=8$ ) before  
 129 euthanasia; in 22 mo group: mice received labels at 2d ( $n=10$ ), 4d ( $n=4$ ), 8d ( $n=9$ ), or 16d ( $n=9$ ) before  
 130 euthanasia. All mice received two labels. Mice were euthanized at 5 or 22 months of age via isoflurane  
 131 inhalation followed by cervical dislocation.



132  
 133 **Figure 2.** Schematic of study experimental procedures. A) Each group of mice received intraperitoneal injections of  
 134 fluorochrome labels at two specific dates (16d, 8d, 4d, or 2d) before euthanasia at either 5 months or 22 months of  
 135 age. B) The femur diaphysis (A/P/M/L regions) and distal metaphysis were imaged with a confocal microscope in  
 136 fluorescence and reflectance modes to evaluate labeled and unlabeled lacunae on the bone surface. Representative  
 137 images show 2d calcein labels (yellow) and 8d alizarin labels in (blue) for 5 mo mice. C) Cortical bone was visually  
 138 divided into lamellar and non-lamellar compartments for further analyses. Cortical bone was also divided into three  
 139 intracortical sections for analysis based on variation in tissue strain. D) MMP14<sup>+</sup> lacunae were counted to quantify  
 140 perilacunar bone resorption for cortical bone. White arrows show MMP14<sup>+</sup> lacunae and black arrows show unlabeled  
 141 lacunae.

## 142 2.2 Sample preparation

143 Right femurs were harvested, cut transversely in half at the femoral midshaft, and then the proximal  
 144 and distal fragments were embedded in non-infiltrating epoxy (Epoxicure 2, Buehler) without any ethanol  
 145 dehydration steps, air-drying, or fixation. The proximal side of the mid-shaft cross-section was used for  
 146 cortical bone studies. The embedded distal halves were cut through the sagittal plane to expose femoral  
 147 metaphysis for cancellous bone studies, using a low-speed diamond saw (Isomet, Buehler). All samples  
 148 were polished to achieve a mirror-like finish, using wet silicon carbide papers (600 and 1000 grits,  
 149 Buehler) followed by Rayon fine cloths and alumina pastes (9, 5, 3, 1, 0.5, 0.3, and 0.05  $\mu\text{m}$ , Ted Pella,  
 150 Inc.).

151 Left femurs were harvested and immediately fixed with 10% neutral-buffered formalin, decalcified  
152 with EDTA disodium salt dihydrate, dehydrated in a graded ethanol series, embedded in paraffin,  
153 transversely cut at femoral midshaft, and each half was serially sliced into 5-micron-thick horizontal  
154 cortical diaphysis sections for immunohistochemistry analyses.

155

### 156 **2.3 Analysis of bone-mineralizing osteocytes via fluorochrome labeling**

157 An inverted confocal laser scanning microscope (CLSM- Leica Stellaris DMI8, Wetzlar, Germany)  
158 was used to identify labeled and unlabeled osteocyte lacunae using a 20× lens (dry, 0.75 NA, 0.78 μm  
159 lateral resolution) at 600 Hz speed with a 1024 × 1024 resolution, and pinhole set at 1 Airy unit. Calcein  
160 labels were visualized using an excitation wavelength of 488 nm and emission wavelength of 500–540  
161 nm. Alizarin labels were visualized using an excitation wavelength of 561 nm and emission wavelength  
162 of 600–645 nm. The reflectance mode was used to image the bone surface, allowing measurement of the  
163 total number of lacunae. Then, fluorescence images were taken from the same site to measure the number  
164 of fluorochrome-labeled lacunae. The percentage of fluorochrome-labeled lacunae on the bone surface  
165 was calculated as the ratio of labeled lacunae to all lacunae on the bone surface (**Figure 2B**). All images  
166 were collected in z-stacks (~30 μm thickness, 0.6 μm between slices) to confirm whether the surface-  
167 visible lacunae were labeled or not in 3D space. For each channel (alizarin and calcein) in every image,  
168 we calculated the mean and standard deviation of the grayscale intensity using ImageJ<sup>42</sup>. Then, we  
169 determined a minimum intensity value by adding 1.5 times the standard deviation to the mean grayscale  
170 intensity. Using Imaris 9.3, we set the minimum threshold of fluorescent intensity for each channel in  
171 each image to this calculated value.

172 The percentage of bone-mineralizing osteocytes (i.e., labeled lacunae) was measured for cortical bone  
173 within anterior (A), posterior (P), medial (M) and lateral (L) regions of interest (ROIs) at the femoral  
174 midshaft (**Figure 2B**). For each ROI, this percentage was also separately reported for lamellar and non-  
175 lamellar compartments of cortical bone, which were visually identified from reflectance images, (**Figure**  
176 **2C**), to assess the impact of different bone types on bone-mineralizing osteocytes.

177 We also investigated the effect of natural strain variations that exist in cortical femur diaphysis<sup>43</sup> on  
178 osteocyte bone mineralization activity. First, we compared the percentage for bone-mineralizing  
179 osteocytes between anterior (close to femur loading axis) and medial (close to femur neutral axis) ROIs  
180 (**Figure 6A**). These quadrants were chosen because the anterior femur experiences tensile strains while  
181 the medial quadrant experiences consistently lower strains. By contrast, the posterior and lateral quadrants  
182 experience more complicated stresses<sup>43</sup>. Because tensile strains increase from the endocortical to  
183 periosteal surfaces of the anterior quadrant<sup>43</sup>, we also compared the percent of bone mineralizing lacunae  
184 with respect to intracortical position with relation to the endocortical surface: 0-30%, 30-70%, and 70-

185 100% of the cortical thickness (**Figure 2C**). We referred to the sections as Ec (endocortical, 0-30%), Mid  
186 (middle, 30-70%), and Ps (periosteal, 70-100%). These same regions were also assessed for the medial  
187 quadrant, which has much less intracortical stress variation<sup>43</sup>. For analyses of cancellous bone, multiple  
188 trabecular regions (**Figure 2B**) were selected from the metaphysis of each mouse, exposed by sagittal  
189 sectioning of the femur's distal half. The percentage of labeled lacunae was calculated for each trabecular  
190 region (**Figure 2B**), and then the mean and standard deviation of all trabecular regions in each mouse  
191 were reported. Custom Matlab codes were employed for these analyses (MATLAB codes available on  
192 GitHub repository: [https://github.com/Ghazal-vhd/LCST\\_LabelCount\\_Femur.git](https://github.com/Ghazal-vhd/LCST_LabelCount_Femur.git)). These codes counted  
193 the number of lacunae on the bone surface from reflective images and the number of labeled lacunae from  
194 fluorescence images within regions of interest defined by the user, calculating the percentage of labeled  
195 lacunae for both cortical and cancellous regions.

196 During data collection, the laser for the Leica Stellaris DMI8 was updated from a diode laser to a  
197 white light laser while the detectors remained unchanged. Emission and excitation ranges were kept  
198 similar, but adjustments were made to the new laser's settings such as gain and power to ensure a uniform  
199 image production. All images, both pre- and post-update, were normalized to their respective mean and  
200 variable intensity, as previously described. Our analysis revealed no discernible impact of the laser  
201 change (included as a blocking factor in all the statistical models) on any outcomes.

202 The high-resolution images in **Figure 1** were from cortical femurs of a 5 months old female  
203 C57BL/6JN mouse. This mouse received alizarin injection 8 days and calcein injection 2 days before  
204 euthanasia. Both femurs were dehydrated with degraded ethanol series and embedded in polymethyl  
205 methacrylate. The right femur was stained with basic fuchsin during the dehydration process<sup>44,45</sup> and used  
206 for **Figure 1A**. Images were taken with a 63×-oil immersion objective using the same Leica Stellaris  
207 DMI8 confocal microscope.

208

## 209 **2.4 Analysis of osteocyte matrix metalloproteinase expression by immunohistochemistry**

210 Paraffin-embedded left distal femurs were used for immunohistochemistry (IHC) following  
211 previously published protocols<sup>46</sup>. Slides were dewaxed and rehydrated (ethanol and distilled water series).  
212 Subsequently, the slides were incubated in Innovex Uni-Trieve retrieval solution (329ANK, Innovex  
213 Animal IHC kit) for 30 min in a 65 °C water bath. Slides were blocked with the Innovex kit's Fc-block  
214 and Background Buster, each for 45 minutes in the room temperature. Next, samples were incubated with  
215 the primary antibodies (1:100 anti-MMP14; ab38971 both diluted in PBS) for one hour at room  
216 temperature and subsequently with secondary antibodies (Linking Ab, 329ANK) and peroxidase (HRP)  
217 enzyme for 10 minutes each at room temperature. Following this, the slides were treated with DAB  
218 working solution at room temperature for 5 minutes, washed with PBS, and mounted with Innovex

219 Advantage permanent mounting media. Negative controls were conducted by replacing the primary  
220 antibody with rabbit IgG at the same concentration. Images were captured using a Nikon E-50i  
221 microscope (Nikon, Melville, NY, SA) with dry 4× (full cortical cross-section) and dry 20× (each cortical  
222 ROI) objectives (**Figure 2D**). For MMP14 comparisons, we had n=18 and n=20 mice for 5 mo and 22 mo  
223 groups, respectively. The mean percentage of MMP14+ osteocyte lacunae for each cortical ROI (A, P, M  
224 and L) was quantified using ImageJ. This percentage was not characterized in cancellous bone due to  
225 sample availability.

226

## 227 **2.5 Analysis of lacunar geometry via scanning electron microscopy**

228 A subset of samples (n=6 per age) was coated with a thin layer of carbon for lacunar geometrical  
229 analyses via backscattered scanning electron imaging (Zeiss Supra 55VP field emission SEM, 15 kV,  
230 60 μm aperture size, 400× magnification, and 9.1 mm working distance). Samples were mounted in a  
231 custom holder that ensures flat surfaces at the same height<sup>47</sup>. Images were collected for the anterior ROI.  
232 A custom Matlab code was used to calculate lacunar geometry for the lamellar compartment of cortical  
233 bone<sup>16</sup>. An area filter removed objects smaller than ~5 μm<sup>2</sup> and larger than ~200 μm<sup>2</sup>. Then, pores  
234 smaller than ~70 μm<sup>2</sup> were considered lacunae. The following parameters were calculated: lacunar  
235 porosity (%), lacunar number density (#/ mm<sup>2</sup>), lacunar area (μm<sup>2</sup>, the area of an ellipse fitted to the  
236 segmented 2D osteocyte lacunae), lacunar major and minor axes (μm), and lacunar circularity (i.e., ratio  
237 of minor to major axis of the fitted ellipse, where a value of 1 indicates a perfect circle). We also assessed  
238 differences in lacunar geometry between labeled and unlabeled lacunae for a small subset of samples that  
239 were labeled 8 days and 2 days before euthanasia in both 5 mo (n=4) and 22 mo (n=3) groups. We  
240 overlapped the SEM images with CLSM maps of labeled and unlabeled lacunae to test whether lacunar  
241 area differs between bone-mineralizing and non-bone-mineralizing osteocytes.

242

## 243 **2.6 Statistical analyses**

244 Mixed model ANOVA, with mouse as the random effect, tested whether percentage of bone-  
245 mineralizing osteocytes depended on the fixed effects of age, tissue strain (i.e., A/P/M/L ROIs), label  
246 date, or interactions of these variables for cortical bone. Additional mixed model ANOVAs were utilized  
247 for lamellar and non-lamellar cortical compartments. For the comparisons of intracortical distances (0-  
248 30%, 30-70%, and 70-100%), the two age groups were separated and for each age, mixed model ANOVA  
249 with mouse as a random effect was used to test if the percentage of bone-mineralizing osteocytes (for 2d  
250 and 16d labels, separately) depended on the fixed effects of ROI, intracortical distance, or their  
251 interactions. For cancellous bone, two-way ANOVA was employed to test if age, label date, and the  
252 interaction of these factors affect percentage of bone-mineralizing osteocytes. Since the confocal laser

253 was changed mid-study, this was included as a blocking factor in these models. Because the laser change  
254 was not a significant effect for any measure, this blocking factor was removed, and models were rerun.  
255 Mixed model ANOVA with mouse as a random effect was used to test if the percentage of MMP14+  
256 lacunae depends on age, ROI, or their interactions. We tested the effect of age on the measurements of  
257 lacunar geometry from SEM using a two-sample t-test. For the lacunar area differences between labeled  
258 and not labeled lacunae, we employed mixed model ANOVA with mouse as the random effect and age  
259 and label status (yes or no) as fixed effects. For all models, model residuals were checked for satisfaction  
260 of assumptions of normality and homoscedasticity. Dependent variables were log-transformed if  
261 necessary to satisfy these assumptions. Significance was set a priori to  $p < 0.05$ . Significant interactions  
262 between factors were followed up with Tukey post hoc tests. All analyses were performed with Minitab  
263 (20).

264

### 265 **3.0 Results**

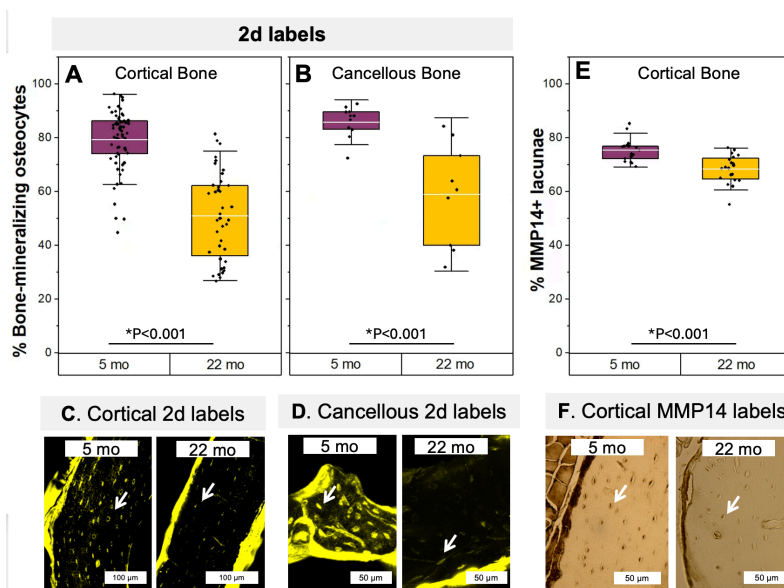
#### 266 **3.1 Aging decreases the number of osteocytes participating in peri-LCS turnover**

267 Osteocyte participation in mineralizing their immediate surrounding was highly abundant in the  
268 cortical and cancellous femur of young adult C57BL/6JN mice. However, with aging, there was a large  
269 decrease in the percentage of recently bone-mineralizing osteocytes (i.e., 2d labeled lacunae) in both  
270 cortical and cancellous regions. In cortical bone of 5 mo mice, 80% of lacunae showed 2d labels, while in  
271 22 mo mice, 50% of lacunae had 2d labels. Thus, from 5 mo to 22 mo, there was a 38% reduction in the  
272 percentage of 2d labeled lacunae in cortical bone ( $p < 0.001$ , **Figure 3A & C**). In cancellous bone of 5 mo  
273 mice, 85% of the lacunae had 2d labels, while in 22 mo mice, 58% of lacunae showed 2d labels.  
274 Therefore, aging reduced the percentage of 2d labeled lacunae by 32% ( $p < 0.001$ , **Figure 3B & D**).

275 The percentage of double-labeled lacunae (i.e., positive for both 2d and 16d labels) was also abundant  
276 in 5 mo femurs, with more than 45% of the lacunae in cortical bone and 60% of lacunae in cancellous  
277 bone having double-labels. The percentage of double-labeled lacunae decreased with aging. In 22 mo  
278 mice, 26% of lacunae in cortical bone and 10% of lacunae in cancellous bone showed double-labels.  
279 Thus, from 5 mo to 22 mo, there were 45% ( $p = 0.05$ , **Figure S2**) and 85% ( $p < 0.001$ , **Figure S2**) fewer  
280 double-labeled lacunae in cortical and cancellous tissues, respectively.

281 The percentage of MMP14+ lacunae (i.e., positive for a marker of bone resorption) was also highly  
282 abundant in femoral cortical bone of 5 mo mice. For these young adult mice, more than 75% of cortical  
283 lacunae were positive for MMP14 (**Figure 3E & F**). With increased age, there was a significant decrease  
284 in the percentage of MMP14+ lacunae (22 mo vs 5 mo: -10%,  $p < 0.001$ ). The percentage of MMP14+  
285 lacunae was not characterized in cancellous bone due sample availability and future investigations would  
286 benefit from this analysis.

287 Our data showed greater variability in the percentage of bone mineralizing osteocytes in both cortical  
 288 and cancellous bones of 22 mo mice compared to 5 mo mice (SD comparisons of 22 mo vs 5 mo groups;  
 289 Cortical: +60%,  $p < 0.05$ ; Cancellous: +230%,  $p < 0.001$ ;  $p$  values are from Bartlett and Levene tests of  
 290 equality of variances between the two groups). This is consistent with observations of higher variability in  
 291 bone matrix quality and LCS characteristics with aging<sup>16,48-52</sup>.  
 292



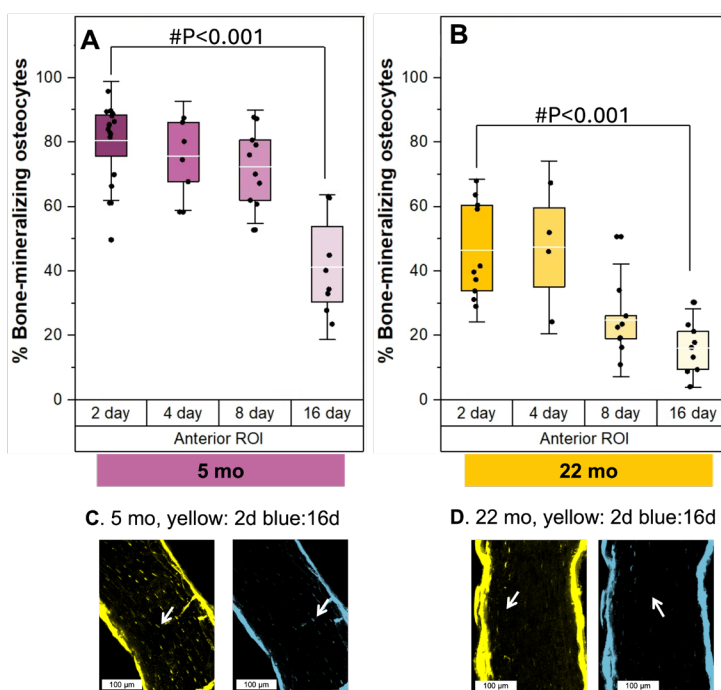
293  
 294 **Figure 3.** The effect of aging on cortical and cancellous osteocyte bone mineralization and resorption. Bone-  
 295 mineralizing osteocytes were less abundant with aging in both A) cortical and B) cancellous bone. Only 2d labels are  
 296 shown here. C & D) Representative fluorescence images of calcein labels for 5 mo and 22 mo mice shown. For 2d  
 297 label comparisons, we had  $n=16$  and  $n=10$  mice for 5 mo and 22 mo groups, respectively. E & F) Aging also decreased  
 298 the percentage of MMP14+ lacunae in cortical bone. White arrows show 2d labeled (yellow) or MMP14+ lacunae.  
 299 All data are reported as percentages (labeled lacunae/all lacunae). For MMP14 comparisons, we had  $n=18$  and  $n=20$   
 300 mice for 5 mo and 22 mo groups, respectively. Boxplots represent mean value (cross), interquartile range (box),  
 301 minimum/maximum (whiskers), and symbols representing all data points. All  $p$ -values correspond with results of the  
 302 omnibus ANOVA test. \* indicates a significant effect of age.

### 303 3.2 Aging alters peri-LCS turnover dynamics more for cancellous than for cortical bone

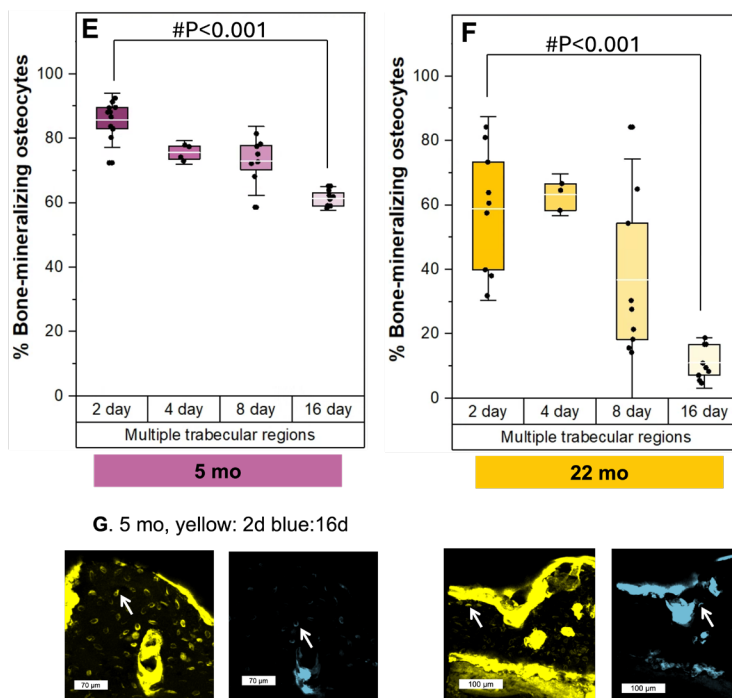
304 The percentage of labeled lacunae decreased for injection dates further from euthanasia. For  
 305 cancellous bone from 5 mo mice, the percentage of 16d labeled lacunae was 29% ( $p < 0.001$ ) lower  
 306 compared to 2d labeled lacunae (**Figure 4E & G**). By contrast, at 22 mo, the percentage of 16d labeled  
 307 lacunae was 81% ( $p < 0.001$ ) lower compared to 2d labeled lacunae (**Figure 4F & H**), suggesting that the  
 308 rate of label disappearance is higher with increased age in cancellous bone. In cancellous bone of both 5  
 309 mo and 22 mo groups, the percentage of 8d labels decreased compared to 2d labels (5 mo: -15%,  $p <$   
 310 0.001, 22 mo: -39%,  $p < 0.001$ ), while the percentage of 4d labels was not different from 2d labels ( $p >$   
 311 0.05).

312 In cortical bone of 5 mo mice, there were 44% ( $p < 0.001$ ) fewer lacunae labeled at 16d compared to  
313 2d (**Figure 4A & C**). For 22 mo mice, there were 61% ( $p < 0.001$ ) fewer 16d labeled lacunae compared  
314 to 2d labeled lacunae (**Figure 4B & D**), implying that in cortical bone, peri-LCS turnover undergoes a  
315 more modest change with aging compared to cancellous bone. There were 47% ( $p < 0.001$ ) fewer lacunae  
316 with 8d labels compared to 2d labels in cortical bone of 22 mo mice, however, 8d label percentage was  
317 not different from 2d label percentage in 5 mo mice ( $p > 0.05$ ). The percentage of 4d labels was not  
318 different from 2d labels ( $p > 0.05$  for either age).  
319

## Cortical Bone



## Cancellous Bone



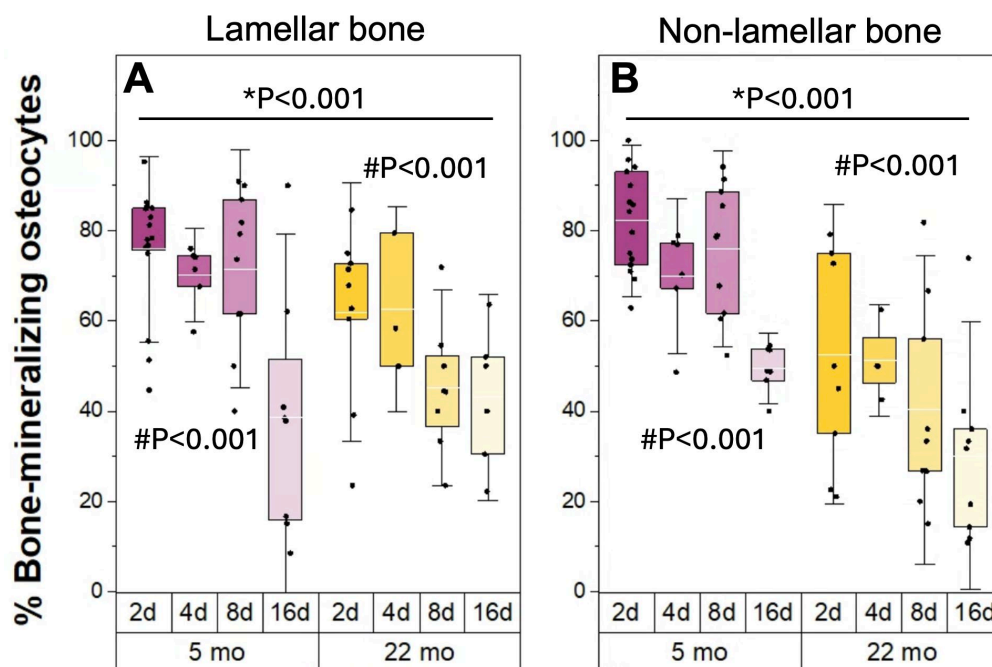
320

321 **Figure 4.** The effect of aging on the dynamics of osteocyte bone turnover. A-D) In cortical bone, compared to 2d  
 322 labels, labels administrated 16d before euthanasia were 44% and 61% less abundant in 5 mo and 22 mo mice,  
 323 respectively. E-H) In cancellous bone, compared to 2d labels, 16d labels were 29% and 81% less abundant in 5 mo  
 324 and 22 mo mice, respectively, suggesting aging alters peri-LCS turnover dynamics more for cancellous than for  
 325 cortical bone. Data for other ROIs of cortical bone are shown in supplementary information. All data are reported as  
 326 percentages (labeled lacunae/all lacunae). Representative fluorescence images of 2d labels (calcein label is shown in

327 yellow) and 16d labels (alizarin label is shown in blue) for 5 mo and 22 mo samples shown in both cortical and  
 328 cancellous tissues. White arrows show 2d labeled lacunae. For the 5 mo group, sample sizes were: 2d (n=16), 4d  
 329 (n=6), 8d (n=10), and 16d (n=8). For 22 mo group, sample sizes were: 2d (n=10), 4d (n=4), 8d (n=9), and 16d (n=9).  
 330 Boxplots represent mean value (cross), interquartile range (box), minimum/maximum (whiskers), and symbols  
 331 representing all data points. All p-values correspond with results of the omnibus ANOVA test. # indicates a significant  
 332 effect of injection date.

### 333 3.3 The impact of aging on peri-LCS turnover is similar between lamellar and non-lamellar 334 compartments of cortical bone

335 Since osteocyte lacunar geometry depends on the bone structural organization (e.g., lamellar vs non-  
 336 lamellar bone)<sup>40,41</sup>, we further divided the cortical bone into lamellar and non-lamellar compartments. We  
 337 observed a similar age-induced decline in the percentage of bone-mineralizing osteocytes in both lamellar  
 338 (for M ROI, 22 mo vs 5 mo: -49%,  $p < 0.001$ ) and non-lamellar (for M ROI, 22 mo vs 5 mo: -46%,  $p <$   
 339  $0.001$ ) bones (**Figure 5**, **Figure S3** shows data for all ROIs). Similarly, in both age groups, 16d labels  
 340 were significantly less abundant compared to 2d labels in both lamellar (for M ROI, 5 mo 16d vs 2d: -  
 341 40%, 22 mo 16d vs 2d: -62%, all  $p < 0.001$ ) and non-lamellar compartments (for M ROI, 5 mo 16d vs 2d:  
 342 -45%, 22 mo 16d vs 2d: -60%, all  $p < 0.001$ ) of cortical bone (**Figure 5**).



343  
 344 **Figure 5.** The effect of aging is similar in reducing LCS bone mineralization for both lamellar and non-lamellar  
 345 bone. For both A) lamellar and B) non-lamellar compartments of cortical bone, aging reduced the percentage of  
 346 bone-mineralizing osteocytes. For both types of tissues, 16d labeled lacunae were significantly less abundant  
 347 compared to 2d labeled lacunae regardless of the age group. Data are shown for the medial ROI, where we  
 348 consistently observed comparable amounts of both lamellar and non-lamellar bone across all mice. In contrast, the  
 349 size of lamellar and non-lamellar bone regions varied significantly in the other ROIs, and some mice did not have  
 350 non-lamellar bone in the anterior ROI. Results for all ROIs are presented in Figure S3. All data are reported as  
 351 percentages (labeled lacunae/all lacunae). Boxplots represent mean value (cross), interquartile range (box),

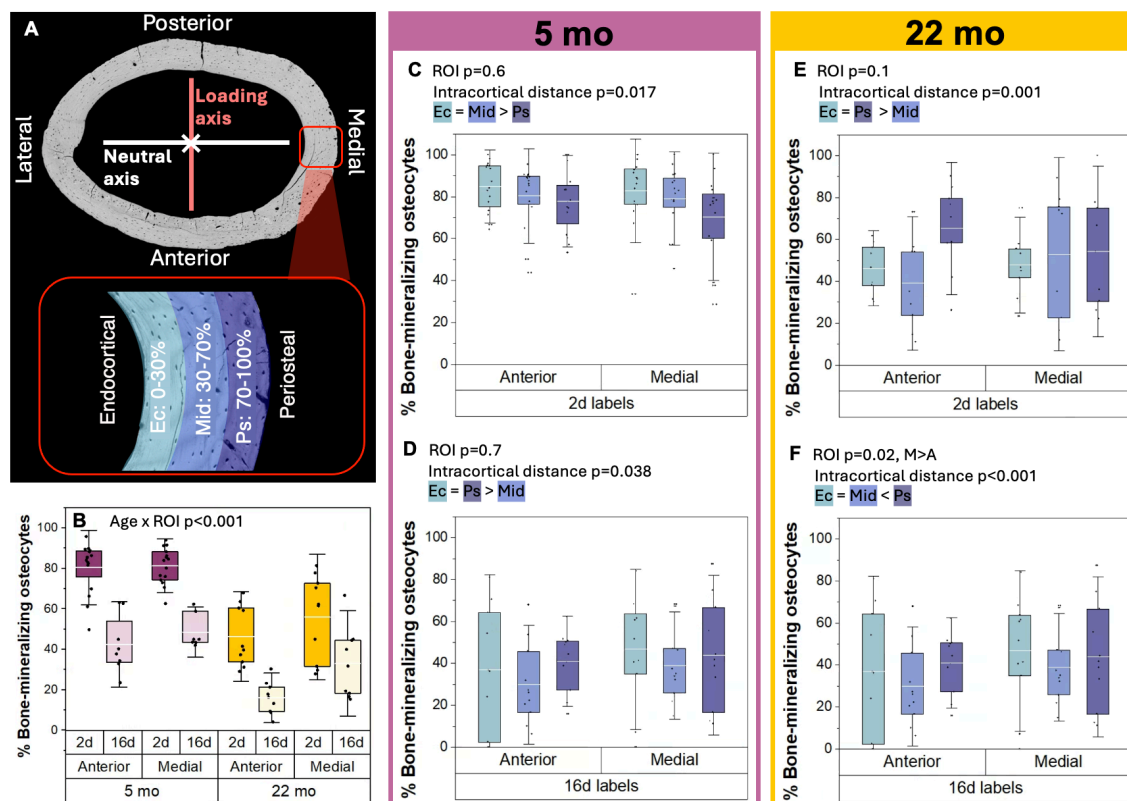
352 minimum/maximum (whiskers), and symbols representing all data points. All p-values correspond with results of  
353 the omnibus ANOVA test. \* indicates a significant effect of age. # indicates a significant effect of injection date.

### 354 **3.4 The relationship between peri-LCS turnover and cortical quadrant and intracortical location of** 355 **osteocytes depends on age**

356 In mouse femur cross-section, the strain environment is distinct between anterior (A), posterior (P),  
357 medial (M), and lateral (L) ROIs based on their position with respect to the femur loading axis and natural  
358 axis (**Figure 6A**)<sup>43</sup>. Because the osteocyte is a mechanosensitive cell<sup>38,39</sup>, we compared LCS bone  
359 mineralization and resorption for these ROIs. In 5 mo mice, we did not find a relationship between LCS  
360 turnover dynamics and the position of the osteocytes in distinct strain environments of the femur cortex ( $p$   
361 = 0.815, **Figure 6B**). However, in 22 mo mice, we found an association between the peri-LCS turnover  
362 dynamics and the position of the osteocytes in different ROIs of cortical femur (age and ROI interaction  $p$   
363 < 0.001). Osteocytes in the medial ROI of aged femurs (close to femur neutral axis) had higher  
364 participation in mineralizing their surrounding compared to those in the other three ROIs (e.g., M vs A:  
365 +44%  $p < 0.001$ , **Figure 6B**). There were no differences in the percentage of labels among anterior,  
366 posterior, and lateral ROIs. Notably, the decay of 16-day labels exhibited a slower pace in the medial ROI  
367 in comparison to the others. ROI did not impact the percentage of MMP14+ lacunae in 5 mo or 22 mo  
368 mice ( $p = 0.7$ ).

369 Ascenzi *et al.* demonstrated that for the anterior ROI of the mouse femur, intracortical tissue tensile  
370 strains increases with distance from the centroid<sup>43</sup>. However, in the medial ROI, which is close to the  
371 femur neutral axis, strains are lower and are relatively unaffected by distance from the centroid. The  
372 intracortical strain distribution is more complex for posterior and lateral ROIs<sup>43</sup>. Therefore, we divided  
373 anterior and medial ROIs with simpler and more distinct strain distribution patterns into three sections  
374 with respect to the position between the endocortical and periosteal surfaces. Distance sections included  
375 Ec: 0-30%, Mid: 30-70%, and Ps: 70-100% (**Figure 6A**). There were no significant interactions between  
376 ROI and distance for either 5 mo or 22 mo mice. In 5 mo mice, both 2d labeled and 16d labeled lacunae  
377 percentages were influenced by the intracortical position but not by ROI. At this age, posthoc testing  
378 reveals that the lacunae closest to the periosteal surface (Ps: last 70-100% of cortical thickness) had a  
379 smaller percentage of 2d labels compared to the other two distances (Ec = Mid > Ps,  $p = 0.017$ , **Figure**  
380 **6C**). There were fewer 16d-labeled lacunae within the middle distance (Mid: 30-70% of cortical  
381 thickness) compared to other distances (Ec = Ps > Mid,  $p = 0.038$ , **Figure 6D**). Differences in the  
382 percentage of labeled lacunae with intracortical position were more pronounced for 22 mo mice. At this  
383 age, lacunae within the middle intracortical distance had lower percentage of 2d labels compared to other  
384 the other distances (Ec = Mid > Ps,  $p = 0.001$ , **Figure 6E**). Periosteal distance section in 22 mo mice

385 showed the highest percentage of 16d labels compared to the other distances (Ec = Mid < Ps,  $p < 0.001$ ,  
 386 **Figure 6F**).  
 387



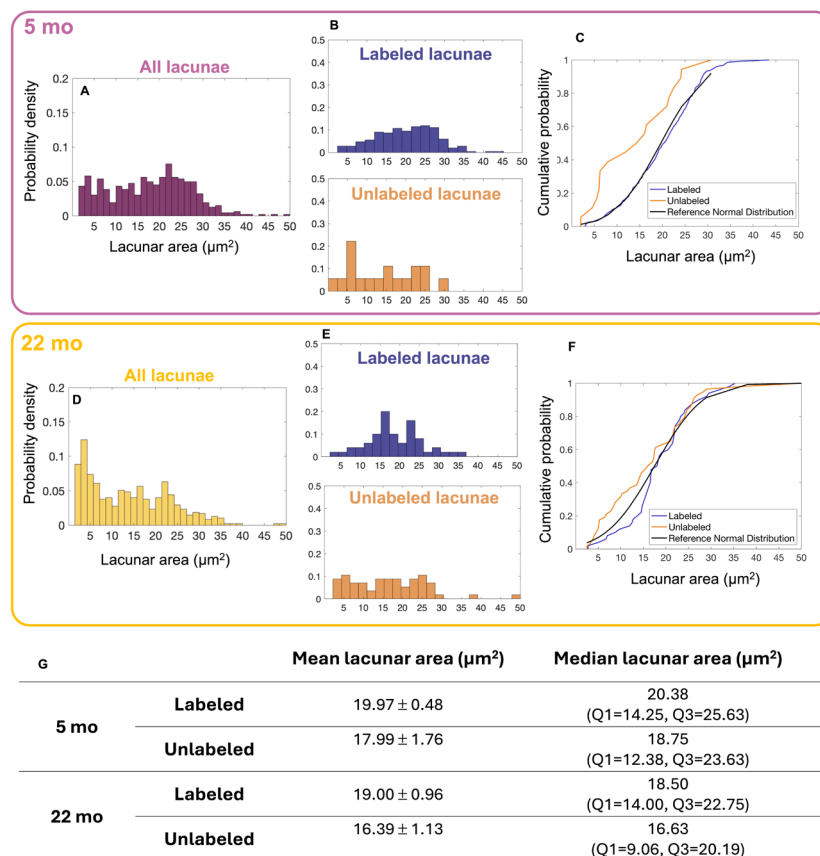
388  
 389 **Figure 6.** Associations between tissue strain and osteocyte participation in LCS bone mineralization. A) Schematic  
 390 of anterior, posterior, medial, and lateral ROIs and their position with respect to the femur loading axis and natural  
 391 axis. Anterior and medial ROIs were divided into three distance sections from the endocortical surface (0-30%, 30-  
 392 70%, and 70-100% of cortical thickness) for further investigation of whether osteocyte bone mineralization  
 393 is associated with differences in tissue strain. B) In 5 mo mice, anterior vs medial ROI did not impact the percentage of  
 394 bone-mineralizing osteocytes. However, for 22 mo mice, lacunae in the medial ROI had the highest percentage of  
 395 labeling compared to all ROIs. C) In 5 mo mice, the percentage of 2d labeled lacunae was lowest in the region closest  
 396 to periosteal surface, for both anterior and medial ROIs. D) For 5 mo mice, the percentage of 16d labeled lacunae  
 397 was lowest in the middle intracortical region, for both anterior and medial ROIs. E) In 22 mo mice, the percentage  
 398 labeling differences between intracortical sections were larger. Middle intracortical section in 22 mo mice had fewer 2d  
 399 labeled lacunae compared to other sections in both anterior and medial ROIs. F) In 22 mo mice, the percentage of 16d  
 400 labeled lacunae was highest in the region closest to periosteal surface and 16d labels consistently showed higher percentages  
 401 in the medial ROI compared anterior ROI. Data are reported as percentages (labeled lacunae/all lacunae). Boxplots  
 402 represent mean value (cross), interquartile range (box), minimum/maximum (whiskers), and symbols representing all  
 403 data points. All  $p$ -values correspond with results of the omnibus ANOVA test.

### 404 3.5 Osteocytes with active peri-LCS turnover have larger lacunae

405 We conducted a quantitative analysis of backscattered SEM images at the anterior ROI of femoral  
 406 cross-sections to assess whether lacunar geometry changes with aging and the recency of labeling. Since  
 407 lacunar geometry differs between lamellar and non-lamellar bones, and the relative size of these regions  
 408 changes in aging, we restricted our analyses to lamellar bone. We chose the anterior ROI because,

409 compared to other ROIs, it was consistently composed mostly of lamellar bone. Compared with 5 mo  
 410 mice, 22 mo mice had decreased cortical lacunar porosity (-27%,  $p=0.037$ ) but not lacunar number  
 411 density ( $p=0.35$ ) (**Figure S4**). Older mice also had smaller lacunae, as seen by smaller lacunar area (-  
 412 22%,  $p=0.02$ ), major axis (-12%,  $p=0.045$ ), minor axis (-15%,  $p=0.05$ ) (**Figure 7A-B, Figure S4**). No  
 413 changes were seen in lacunar circularity with age. It is noted that previous work found that 2D SEM  
 414 analysis is insufficient to detect expected increased sphericity in lacunae with aging<sup>16</sup>.

415 We also asked whether lacunar size differs between labeled and unlabeled lacunae by overlaying  
 416 SEM and CLSM maps of the anterior region at the cortical midshaft femur for only a subset of SEM  
 417 samples that had 2d and 8d labels. The distribution of labeled lacunar sizes is approximately normal for  
 418 both 5 mo and 22 mo mice (**Figure 7 B & E**). By contrast, the sizes of unlabeled lacunae show closer to a  
 419 uniform distribution for both ages. Our data suggest that recent peri-LCS turnover increases lacunar area  
 420 (**Figure 7 B & E**). Labeled lacunae had larger mean (+11% in 5 mo and +14% in 22 mo, both  $p = 0.05$ )  
 421 and median lacunar areas compared with unlabeled lacunae (**Figure 7 A & D & G**).  
 422



423  
 424 **Figure 7.** Osteocytes with active mineralization have larger lacunae. Overlaid SEM and CLSM maps show that A-  
 425 G) labeled lacunae had larger areas compared to unlabeled lacunae in both age groups. A-C) The distribution of lacunar  
 426 sizes in 5 mo mice ( $n=4$ ) was approximately normal for labeled lacunae (i.e., 2d labeled and/or 8d labeled). However,

427 the distribution of lacunar sizes for unlabeled lacunae (i.e., no 2d or 8d labels) deviated from normality. D-F) In 22  
428 mo mice (n=3), labeled lacunae had a distribution of lacunar sizes that was closer to normal whereas unlabeled lacunae  
429 did not have a normal distribution. The distributions in E-F are depicted as probability density function as well as  
430 cumulative density function plots. Data in table are represented as mean with standard error and median with first and  
431 third quartiles.

#### 432 **4.0 Discussion**

433 Osteocyte lacunar-canalicular system (LCS) turnover has been of high research interest as a possible  
434 contributor to age-related changes in bone fracture resistance<sup>2,3,11,12,17,26</sup>. Extensive evidence indicates  
435 that age reduces osteocyte viability and mechanosensitivity<sup>7-10,13,17</sup> and truncates lacunar and canalicular  
436 dimensions and connectivity<sup>11-16</sup>. These changes imply that there is a decrease in peri-LCS turnover in  
437 aging, which could have impacts to osteocyte mechanosensitivity and bone matrix quality<sup>11,13,14,17,27,28</sup>. At  
438 present, however, more questions than answers exist about where and how often osteocytes remove and  
439 replace their surrounding bone. Our study aimed to test the hypothesis that fewer osteocytes participate in  
440 LCS bone mineralization and resorption in aging C57BL/6JN female mice (5 mo vs 22 mo). In this work,  
441 we find that aging reduces cortical and cancellous osteocyte participation in both perilacunar bone  
442 mineralization and resorption, in a manner that likely depends on tissue strain.

443 The osteocyte is known to remove and replace bone surrounding the LCS in response to perturbations  
444 in calcium homeostasis (e.g., lactation, PTH)<sup>11,12,18-25</sup>. However, the participation of osteocytes in peri-  
445 LCS turnover outside of calcium pressure is uncertain<sup>11</sup>. We utilized serial fluorochrome labeling to  
446 estimate where, when, and how often osteocytes turn over their surrounding bone. Each mouse in this  
447 study was administered two fluorochrome labels at different times before euthanasia. We find that  
448 osteocyte bone turnover is highly prevalent in young adult mice, in both cortical and cancellous bone.  
449 Over 80% of osteocytes show fluorochrome labeled lacunae administrated 2 days before euthanasia.  
450 These numbers decrease to around 45% at 16 days before euthanasia, suggesting rapid bone turnover  
451 (**Figure 4**). Since label disappearance is an indirect indicator of bone resorption, we stained decalcified  
452 sections from the contralateral femurs for MMP14. Previous studies suggest that under conditions of  
453 elevated PTH signaling, osteocytes can acidify and demineralize bone matrix using matrix-degrading  
454 enzymes such as cathepsins and matrix metalloproteinases, in a process known as osteocytic  
455 osteolysis<sup>19,22,27</sup>. We show that in 5 mo mice, a comparable percentage of osteocytes are positive for bone  
456 resorption (i.e., MMP14-positive) as for bone mineralization (i.e., fluorochrome-labeled) (**Figure 3**).  
457 Together, these data suggest that osteocytes in the young adult murine skeleton engage in a pattern of  
458 frequent, near-daily bone mineralization along the LCS, coupled with frequent bone resorption events.

459 Aging has established deleterious impacts on the osteocyte. With increased age, osteocyte apoptosis  
460 and senescence both increase while autophagy decreases<sup>5,53</sup>. Aging reduces the size of lacunae and  
461 canaliculi, as well as the connectivity of this network<sup>11-16</sup>. These changes imply, but do not determine,

462 that peri-LCS turnover also changes with age. Here, we report that aging also reduce LCS bone  
463 mineralization and, to a lesser extent, resorption activities. Compared with 5 mo mice, 22 mo mice have a  
464 58% decrease in the percentage of 2d labeled lacunae and a 10% decrease in the percentage of MMP14+  
465 lacunae in cortical bone (**Figure 3**). The rate of decrease in label percentage from 2d to 16d in cortical  
466 bone is similar across ages. These data suggest that while the number of osteocytes participating in peri-  
467 LCS turnover decreases with aging, active osteocytes of different-aged cortical bone may have a  
468 characteristic time span of bone deposition before resorption events. The characteristics of peri-LCS  
469 turnover did not differ between lamellar and non-lamellar bone at either 5 or 22 mo ages. This is an  
470 important finding, since bone organization changes with aging and previous studies have shown that  
471 aging affects LCS geometry and density differently in these bone types<sup>40,54-56</sup>. These data add to our  
472 understanding of aging bone biology by providing the first evidence that peri-LCS turnover activity  
473 declines with aging.

474 Osteocytes reside within cortical and cancellous bone but may have distinct roles within each of these  
475 compartments and different aging-induced impacts in their behaviors. There was a smaller age-related  
476 decline in the percentage of osteocytes engaged in LCS bone mineralization in cancellous versus cortical  
477 bone (-31% vs -58%, **Figure 3**). While the dynamics of bone turnover did not change significantly with  
478 age in cortical bone (i.e., comparable rate of decrease in labeled lacunae from 2d to 16d between ages),  
479 age greatly increased the frequency of bone turnover in cancellous bone (**Figure 4**). These data suggest  
480 that more osteocytes remain active in cancellous bone and may increase their rate of bone turnover  
481 compared with cortical bone. Cancellous bone is known to be more metabolically active than cortical  
482 bone<sup>29-31</sup>. It is possible that cancellous osteocytes have increased burden of participating in calcium  
483 homeostasis in the aging skeleton, but this hypothesis remains speculative at this time.

484 Our data suggest that the smaller lacunae reported in numerous imaging studies of the aging  
485 skeleton<sup>11-16</sup> are associated with decreased osteocyte bone turnover. From coupling scanning electron  
486 microscopy measurements of lacunae with fluorochrome labeling, we find that osteocytes that are  
487 engaged in recent bone mineralization, regardless of the age group, reside within larger lacunae compared  
488 to osteocytes without labels (**Figure 7**). This result suggests that bone resorption events remove a  
489 considerable quantity of bone. It is yet to be fully determined which specific additional factors osteocytes  
490 employ to promote, or inhibit, local bone mineralization and/or formation. For example, it is well  
491 established that osteoblasts participate in local bone mineralization through shuttling hydroxyapatite  
492 precursors in vesicles to be released near forming surfaces<sup>57</sup>. Whether osteocytes engage in these active  
493 mineralization or mineral inhabitation processes should be investigated.

494 The influence of aging on osteocyte peri-LCS turnover may be associated with tissue strain. As an  
495 initial test of this relationship, we assessed changes in peri-LCS turnover with the spatial position of

496 osteocytes within the cortical femur. We tested the association of peri-LCS turnover activities between  
497 the different quadrants of the mouse femoral cross-section, which vary in strain magnitudes and  
498 directions, as well as the variation in intercortical tissue strain with distance from the femoral centroid<sup>43</sup>  
499 (**Figure 6**). In young adult mice, we did not find sufficient evidence to support the hypothesis that peri-  
500 LCS turnover depends on the position of osteocytes within the femur cortex. However, in early old age  
501 mice, we found evidence that osteocyte LCS bone mineralization depends on the position of osteocytes  
502 within the cortical femur. Compared with osteocytes in anterior and posterior regions of cortical bone  
503 (i.e., higher tensile and compressive strains under loading, respectively<sup>38,39</sup>), more osteocytes in the  
504 medial region of aged bones (i.e., closer to neutral axis) were engaged in LCS bone mineralization (i.e.,  
505 highest percentage of 2d labels) and the peri-LCS turnover rate was decreased (i.e., smallest change in the  
506 presence of 16d labels compared to 2d labels). Additionally, for aged mice, there was a stronger  
507 relationship between the position of lacunae within the cortical thickness and peri-LCS mineralization,  
508 where 2d labels were more abundant in both endocortical and periosteal surfaces compared to the middle  
509 section and 16d labels were the most abundant closest to the periosteal surface. These data suggest that  
510 there may be an association between intracortical strain and LCS bone turnover activities that is evident in  
511 aging. However, there are important limitations to this analysis, as the observed spatial interactions with  
512 peri-LCS turnover could be contributed to by factors other than tissue strain, such as specific nutrient  
513 gradients, tissue maturity variations, access to biochemical signals, and differences in shear stress induced  
514 by interstitial fluid flow between different cortical ROIs and intracortical distances<sup>43,58-61</sup>. Future research  
515 needs to determine if and how peri-LCS turnover is associated with changes in skeletal strain, whether  
516 there is a minimum strain required to engage osteocyte peri-LCS turnover, and if this strain threshold  
517 changes with aging.

518 With aging, osteocytes become less mechanosensitive<sup>7-10,13,17</sup>. A persistent question is why aging has  
519 this effect on these long-lived cells. It has been recognized for many years that substantial strain  
520 amplification must occur for osteocytes to respond with anabolic signals to normal skeletal loads<sup>32,62,63</sup>.  
521 The changes in lacunar and canalicular shape with age may reduce tissue strain and fluid flow shear stress  
522 to contribute to these age-related changes in strain experienced by the cell, as shown by several finite  
523 element modeling studies<sup>34,64</sup>. Our data add to this understanding by showing that changes in osteocyte  
524 lacunar size with age are approximately bimodal in distribution (i.e., only some aged osteocytes have  
525 much reduced lacunar size). Further, we show that labeled osteocyte lacunae are larger than non-labeled  
526 lacunae at both ages. Lacunar enlargement with recent peri-LCS turnover activity has been previously  
527 shown under high calcium demands such as lactation or PTH treatment<sup>19,22,24,65</sup>. Our observations suggest  
528 that contributions to osteocyte mechanosensation derived from geometric factors (i.e., shape of lacunae  
529 and canaliculi and the impact of these shape changes on fluid flow) is likely influenced by the activity of

530 these cells in turning over their local bone. Additionally, our prior work demonstrated that labeled  
531 osteocyte lacunae are surrounded by more compliant (i.e., lower modulus) bone<sup>26</sup>. Thus, changes to peri-  
532 LCS turnover in aging have multiple potential avenues for altering strain experienced by osteocytes. Our  
533 result that aging decreases the percentage of osteocytes engaged in LCS bone mineralization and  
534 resorption, but not the apparent rate of label disappearance (i.e., an estimate of resorption), may align with  
535 data from studies on the impact of aging on calcium signaling. In the cortical bone of 22 mo female  
536 C57BL/6JN mice, there are fewer osteocytes (~ -60%) with active calcium signaling compared to  
537 younger mice, yet the remaining osteocytes respond to mechanical load with Ca<sup>2+</sup> peaks of comparable  
538 intensities to those observed in young mice<sup>7</sup>. It is not yet understood whether populations of aged  
539 osteocytes with different LCS bone turnover characteristics vary in their mechanosensitivity. Together,  
540 these data suggest that major gaps still exist in our understanding about the strain experienced by the  
541 osteocyte and how these strains change in aging.

542 Our data also add to the emerging understanding of the osteocyte as a cell with the potential to  
543 directly modify bone matrix properties. Studies on transgenic mice with suppressed TGF- $\beta$  or YAP/TAZ  
544 signaling, or systemic MMP13 deletion, demonstrate that mice with a decreased ability to engage peri-  
545 LCS turnover have more fragile cortical bone<sup>17,27,28,66</sup>. A recent study explored the role of osteocytes in  
546 the loss of bone matrix quality in aging by distinguishing matrix characteristics that decline in aging in a  
547 manner that is either TGF $\beta$ -dependent or -independent. The study demonstrated an essential role for  
548 osteocyte TGF $\beta$  signaling in regulating not only LCS integrity but also collagen material behavior. By  
549 contrast, mineral characteristics were regulated independently of TGF $\beta$  signaling<sup>17</sup>. We add to this  
550 understanding by showing that osteocyte interaction with bone matrix significantly decreases in age. In  
551 addition, our earlier work showed that peri-LCS turnover increases perilacunar bone compliance in both  
552 young adult (5 mo) and early-old-aged (22 mo) mice<sup>26</sup>. Together, these data build an argument towards  
553 the importance of the osteocyte in maintaining bone matrix quality and the decline of these matrix-  
554 regulatory processes in aging.

555 Aging impacts LCS geometry in both humans and rodents, such as decreased lacunar and canalicular  
556 size and connectivity<sup>16,67-70</sup>. If aging also reduces LCS turnover in humans in a similar way that is seen for  
557 mice in this study, the quality of a large amount of bone tissue could be impacted. An adult human  
558 skeleton contains approximately 42 billion osteocytes each with a lacunar surface area of roughly 336  
559  $\mu\text{m}^2$ , compromising a 215  $\text{m}^2$  total surface area<sup>71,72</sup>. From AFM<sup>26</sup> and synchrotron microscopy data<sup>69,73,74</sup>,  
560 the region of bone tissue impacted by LCS turnover might be estimated to extend to about 1 micrometer  
561 from lacunar walls. Assuming a similar reduction from 80% to 50% of osteocytes engaged in LCS  
562 turnover in aging for humans, the amount of bone tissue impacted by this bone turnover would decrease  
563 from 4.7  $\text{m}^2$  to 2.4  $\text{m}^2$ . Importantly, these estimates are only based on peri-lacunar bone turnover and not

564 peri-canalicular bone turnover and are therefore most likely underestimates. Determining peri-LCS  
565 turnover dynamics and the impacts of aging in humans is an important future research direction.

566 There were several important limitations to this study. First, age-related changes in metabolic  
567 processes and LCS network architecture may impact fluorochrome dye uptake between cells in young and  
568 old bones, and this limitation should be addressed in future studies. However, our work provides key  
569 recommendations for measuring the dynamics of LCS bone mineralization. We find that 2d and 4d labels  
570 do not yield statistically significant results across different skeletal sites and ages. In contrast, 8d labels  
571 show differences from 2d labels in aged cortical bones and both ages for cancellous bone, while 16d  
572 labels are consistently lower compared to 2d labels across all groups. We also found that the order of  
573 labeling (calcein first, then alizarin, or vice versa) does not affect the results. In this study, we did not  
574 investigate the impact of aging on LCS bone resorption, as indicated by MMP14+ lacunae, through other  
575 resorption biomarkers such as TRAP, cathepsin K, or MMP13, but this would be valuable in future  
576 investigations. Additionally, our study focused solely on female mice, whereas the literature highlights  
577 important sex differences in osteocyte physiology<sup>17,75</sup>. Moreover, extending the age range of the study  
578 would be beneficial to exploring whether peri-LCS turnover changes during the developmental and  
579 advanced ages. In this study, it was not possible to investigate the age of individual osteocytes in older  
580 bones and discern whether the active osteocytes were young or old.

581 In summary, this study presents the first evidence that osteocyte participation in mineralizing their  
582 surroundings is highly abundant in both cortical and cancellous bone of young adult female C57BL/6JN  
583 mice. In aging, there are fewer osteocytes with active peri-LCS turnover (both bone mineralization and  
584 resorption), yet turnover dynamics remain mostly similar in cortical bone of 5 mo and 22 mo mice,  
585 suggesting that active osteocytes engage in a characteristic peri-LCS turnover response. Our results also  
586 demonstrate that the impacts of aging on peri-LCS turnover are not uniform throughout the femoral  
587 cortex and might differ with tissue strain. The large decline in peri-LCS turnover in aging can have  
588 significant implications for bone quality, since osteocytes with active turnover have larger lacunae in both  
589 age groups as well as more compliant perilacunar tissue<sup>26</sup>. These results together signify a potential role  
590 for osteocyte bone turnover in the loss of bone fracture resistance and changes in mechanosensation in  
591 aging.

592

### 593 **Acknowledgments**

594 This research was made possible by the Department of Mechanical & Industrial Engineering and the  
595 College of Engineering at the Montana State University. This work represents the views of the authors  
596 and not necessarily those of the sponsors. Research reported here is supported by NSF 2120239 and NIH  
597 R03AG068680. Imaging method development and data collection were made possible by the help of Dr.

598 Heidi Smith from the Center for Biofilm Engineering imaging facility at Montana State University,  
599 supported by funding from the National Science Foundation MRI Program (2018562), the M. J. Murdock  
600 Charitable Trust (202016116), the US Department of Defense (77369LSRIP & W911NF1910288), and  
601 by the Montana Nanotechnology Facility (an NNCI member supported by NSF Grant ECCS-2025391).  
602 We thank Dr. Albert Parker for his assistance in statistical analyses. Steven Watson is thanked for his help  
603 with image processing and dissection. Kenna Brown and Connor Devine are thanked for their assistance  
604 with tissue harvest. Grace Roaming, Chloe Woodwall, and Shane Stauffer are thanked for their help with  
605 sample preparation. We thank Fatema Aljamal, Leah Davidson, Torie Prall, Megan Brenna, Kelly Silk,  
606 and Allison Stevens for their help with initial steps of method development for this project. Alexey  
607 Dynkin is appreciated for manuscript proofreading. We thank Montana State University's Animal  
608 Resource Center staff and especially Tamara Marcotte for the help in providing excellent mouse care.

609

#### 610 **Author Contributions**

611 Ghazal Vahidi: Investigation; methodology; data curation; formal analysis; visualization; writing –  
612 original draft; writing – review and editing. Connor Boone: Investigation; methodology; writing – review  
613 and editing. Fawn Hoffman: Formal analysis; Investigation; methodology; writing – review and editing.  
614 Chelsea Heveran: Conceptualization; methodology; formal analysis; resources; project administration;  
615 supervision; writing - original draft; writing - review and editing.

616

617 **Declarations of interest:** none

618 **References**

- 619 1. Ensrud, K. E. Epidemiology of fracture risk with advancing age. *Journals of Gerontology - Series*  
620 *A Biological Sciences and Medical Sciences* **68**, 1236–1242 (2013). 10.1093/gerona/glt092
- 621 2. Bonewald, L. F. The amazing osteocyte. *Journal of bone and mineral research* **26**, 229–238  
622 (2011).
- 623 3. Schaffler, M. B., Cheung, W. Y., Majeska, R. & Kennedy, O. Osteocytes: Master orchestrators of  
624 bone. *Calcif Tissue Int* **94**, 5–24 (2014). PMC3947191
- 625 4. Alliston, T. Biological regulation of bone quality. *Curr Osteoporos Rep* **12**, 366–375 (2014).  
626 10.1007/s11914-014-0213-4
- 627 5. Sherk, V. D. & Rosen, J. Senescent and apoptotic osteocytes and aging : Exercise to the rescue ?  
628 **121**, 255–258 (2019). PMC6459182
- 629 6. Jilka, R. L., Noble, B. & Weinstein, R. S. Osteocyte apoptosis. *Bone* **54**, 264–271 (2013).  
630 PMC3624050
- 631 7. Morrell, A. E., Robinson, S. T., Silva, M. J. & Guo, X. E. Mechanosensitive Ca<sup>2+</sup> signaling and  
632 coordination is diminished in osteocytes of aged mice during ex vivo tibial loading. *Connect*  
633 *Tissue Res* **61**, 389–398 (2020). 10.1080/03008207.2020.1712377
- 634 8. Hemmatian, H., Bakker, A. D., Klein-Nulend, J. & van Lenthe, G. H. Aging, Osteocytes, and  
635 Mechanotransduction. *Curr Osteoporos Rep* **15**, 401–411 (2017).
- 636 9. Razi, H. *et al.* Aging leads to a dysregulation in mechanically driven bone formation and  
637 resorption. *Journal of Bone and Mineral Research* **30**, 1864–1873 (2015).
- 638 10. Holguin, N., Brodt, M. D., Sanchez, M. E. & Silva, M. J. Aging diminishes lamellar and woven  
639 bone formation induced by tibial compression in adult C57BL/6. *Bone* **65**, 83–91 (2014).  
640 10.1016/j.bone.2014.05.006
- 641 11. Heveran, C. M. & Boerckel, J. D. Osteocyte Remodeling of the Lacunar-Canalicular System:  
642 What’s in a Name? *Current Osteoporosis Reports* **21**, 11–20 (2023). 10.1007/s11914-022-00766-3
- 643 12. Vahidi, G., Rux, C., Sherk, V. D. & Heveran, C. M. Lacunar-canalicular bone remodeling:  
644 impacts on bone quality and tools for assessment. *Bone* 115663 (2020).  
645 doi:10.1016/j.bone.2020.115663 10.1016/j.bone.2020.115663
- 646 13. Schurman, C. A., Verbruggen, S. W. & Alliston, T. Disrupted osteocyte connectivity and  
647 pericellular fluid flow in bone with aging and defective TGF- $\beta$  signaling. *Proceedings of the*  
648 *National Academy of Sciences* **118**, e2023999118 (2021). 10.1073/pnas.2023999118/-  
649 /DCSupplemental
- 650 14. Tiede-Lewis, L. A. M. & Dallas, S. L. Changes in the osteocyte lacunocanalicular network with  
651 aging. *Bone* **122**, 101–113 (2019). 10.1016/j.bone.2019.01.025

- 652 15. Tiede-Lewis, L. M. *et al.* Degeneration of the osteocyte network in the C57Bl/6 mouse model of  
653 aging. *Aging* **9**, 2190–2208 (2017). PMC5680562
- 654 16. Heveran, C. M., Rauff, A., King, K. B., Carpenter, R. D. & Ferguson, V. L. A new open-source  
655 tool for measuring 3D osteocyte lacunar geometries from confocal laser scanning microscopy  
656 reveals age-related changes to lacunar size and shape in cortical mouse bone. *Bone* **110**, (2018).  
657 PMC5878731
- 658 17. Schurman, C. A. *et al.* Aging impairs the osteocytic regulation of collagen integrity and bone  
659 quality. *Bone Res* **12**, 13 (2024). 10.1038/s41413-023-00303-7
- 660 18. Kaya, S. *et al.* Lactation-induced changes in the volume of osteocyte lacunar-canalicular space  
661 alter mechanical properties in cortical bone tissue. *Journal of Bone and Mineral Research* **32**,  
662 688–697 (2017). PMC5395324
- 663 19. Qing, H. *et al.* Demonstration of osteocytic perilacunar/canalicular remodeling in mice during  
664 lactation. *Journal of Bone and Mineral Research* **27**, 1018–1029 (2012). 10.1002/jbmr.1567
- 665 20. Lane, N. E. *et al.* Glucocorticoid-treated mice have localized changes in trabecular bone material  
666 properties and osteocyte lacunar size that are not observed in placebo-treated or estrogen-deficient  
667 mice. *Journal of Bone and Mineral Research* **21**, 466–476 (2006). 10.1359/JBMR.051103
- 668 21. Gardinier, J. D., Al-Omaishi, S., Morris, M. D. & Kohn, D. H. PTH signaling mediates perilacunar  
669 remodeling during exercise. *Matrix Biology* **52–54**, 162–175 (2016). PMC4875803
- 670 22. Jähn, K. *et al.* Osteocytes Acidify Their Microenvironment in Response to PTHrP In Vitro and in  
671 Lactating Mice In Vivo. *Journal of Bone and Mineral Research* **32**, 1761–1772 (2017).  
672 10.1002/jbmr.3167
- 673 23. Yajima, A. *et al.* Osteocytic perilacunar/canalicular turnover in hemodialysis patients with high  
674 and low serum PTH levels. *Bone* **113**, 68–76 (2018). 10.1016/j.bone.2018.05.002
- 675 24. Qing, H. & Bonewald, L. F. Osteocyte remodeling of the perilacunar and pericanalicular matrix.  
676 *International journal of oral science* **1**, 59–65 (2009). 10.4248/ijos.09019
- 677 25. Tazawa, K. *et al.* Osteocytic osteolysis observed in rats to which parathyroid hormone was  
678 continuously administered. *J Bone Miner Metab* **22**, 524–529 (2004). 10.1007/s00774-004-0519-x
- 679 26. Rux, C. J., Vahidi, G., Darabi, A., Cox, L. M. & Heveran, C. M. Perilacunar bone tissue exhibits  
680 sub-micrometer modulus gradation which depends on the recency of osteocyte bone formation in  
681 both young adult and early-old-age female C57Bl/6 mice. *Bone* **157**, (2022).  
682 10.1016/j.bone.2022.116327
- 683 27. Tang, S., Herber, R.-P., Ho, S. & Alliston, T. Matrix Metalloproteinase-13 is Required for  
684 Osteocytic Perilacunar Remodeling and Maintains Bone Fracture Resistance SY. *J Bone Miner*  
685 *Res.* **27**, 1936–1950 (2012). 10.1002/jbmr.1646.Matrix

- 686 28. Kegelmann, C. D. *et al.* YAP and TAZ Mediate Osteocyte Perilacunar/Canalicular Remodeling.  
687 *Journal of Bone and Mineral Research* **00**, 1–15 (2019). 10.1002/jbmr.3876
- 688 29. Hadjidakis, D. J. & Androulakis, I. I. Bone remodeling. *Ann N Y Acad Sci* **1092**, 385–396 (2006).
- 689 30. Delmas, P. D. Biochemical markers of bone turnover for the clinical assessment of metabolic bone  
690 disease. *Endocrinol Metab Clin North Am* **19**, 1–18 (1990).
- 691 31. Shahnazari, M. *et al.* Bone turnover markers in peripheral blood and marrow plasma reflect  
692 trabecular bone loss but not endocortical expansion in aging mice. *Bone* **50**, 628–637 (2012).  
693 10.1016/j.bone.2011.11.010
- 694 32. Wang, Y., Mcnamara, L. M., Schaffler, M. B. & Weinbaum, S. *Strain amplification and integrin*  
695 *based signaling in osteocytes*.
- 696 33. Lewis, K. J. *et al.* Estrogen depletion on In vivo osteocyte calcium signaling responses to  
697 mechanical loading. *Bone* **152**, (2021). 10.1016/j.bone.2021.116072
- 698 34. Nazer, R. Al, Lanovaz, J., Kawalilak, C., Johnston, J. D. & Kontulainen, S. Direct in vivo strain  
699 measurements in human bone — A systematic literature review. *J Biomech* **45**, 27–40 (2012).  
700 10.1016/j.jbiomech.2011.08.004
- 701 35. Nicolella, D. P. *et al.* Effects of nanomechanical bone tissue properties on bone tissue strain:  
702 Implications for osteocyte mechanotransduction. *Journal of Musculoskeletal Neuronal*  
703 *Interactions* **8**, 330–331 (2008).
- 704 36. Lai, X., Chung, R., Li, Y., Liu, X. S. & Wang, L. Lactation alters fluid flow and solute transport in  
705 maternal skeleton: A multiscale modeling study on the effects of microstructural changes and  
706 loading frequency. *Bone* **151**, (2021). 10.1016/j.bone.2021.116033
- 707 37. Sang, W. & Ural, A. Quantifying how altered lacunar morphology and perilacunar tissue  
708 properties influence local mechanical environment of osteocyte lacunae using finite element  
709 modeling. *J Mech Behav Biomed Mater* **135**, (2022). 10.1016/j.jmbbm.2022.105433
- 710 38. Rudman, K. E., Aspden, R. M. & Meakin, J. R. Compression or tension? The stress distribution in  
711 the proximal femur. *Biomed Eng Online* **5**, (2006). 10.1186/1475-925X-5-12
- 712 39. Ramasamy, J. G. & Akkus, O. Local variations in the micromechanical properties of mouse femur:  
713 The involvement of collagen fiber orientation and mineralization. *J Biomech* **40**, 910–918 (2007).  
714 10.1016/j.jbiomech.2006.03.002
- 715 40. Bach-Gansmo, F. L. *et al.* Osteocyte lacunar properties in rat cortical bone: Differences between  
716 lamellar and central bone. *J Struct Biol* **191**, 59–67 (2015).  
717 <https://doi.org/10.1016/j.jsb.2015.05.005>

- 718 41. Palumbo, C. & Ferretti, M. *Histomorphometric study on the osteocyte lacuno-canalicular network*  
719 *in animals of different species. I. Woven-fibered and parallel-fibered bones. Article in Italian*  
720 *Journal of Anatomy and Embryology* (1998).
- 721 42. Schneider, C. A., Rasband, W. S. & Eliceiri, K. W. *NIH Image to ImageJ: 25 years of Image*  
722 *Analysis HHS Public Access. Nat Methods* **9**, (2012).
- 723 43. Ascenzi, M. G. *et al.* Hyperlipidemia affects multiscale structure and strength of murine femur. *J*  
724 *Biomech* **47**, 2436–2443 (2014). 10.1016/j.jbiomech.2014.04.006
- 725 44. Poundarik, A. A. & Vashishth, D. Multiscale imaging of bone microdamage. *Connect Tissue Res*  
726 **56**, 87–98 (2015). 10.3109/03008207.2015.1008133
- 727 45. Burr, D. B. & Hooser, M. *Alterations to the En Bloc Basic Fuchsin Staining Protocol for the*  
728 *Demonstration of Microdamage Produced In Vivo. Bone* **17**, (1995).
- 729 46. Hilton, M. J. *Skeletal Development and Repair*. (Springer, 2016).
- 730 47. Vahidi, G. *et al.* Germ-Free C57BL/6 Mice Have Increased Bone Mass and Altered Matrix  
731 Properties but Not Decreased Bone Fracture Resistance. *Journal of Bone and Mineral Research*  
732 **38**, 1154–1174 (2023). 10.1002/jbmr.4835
- 733 48. Milovanovic, P. & Busse, B. Inter-site variability of the human osteocyte lacunar network:  
734 implications for bone quality. *Curr Osteoporos Rep* **17**, 105–115 (2019).
- 735 49. Ashique, A. M. *et al.* Lacunar-canalicular network in femoral cortical bone is reduced in aged  
736 women and is predominantly due to a loss of canalicular porosity. *Bone Rep* **7**, 9–16 (2017).  
737 10.1016/j.bonr.2017.06.002
- 738 50. Paschalis, E. P. *et al.* Aging Versus Postmenopausal Osteoporosis: Bone Composition and  
739 Maturation Kinetics at Actively-Forming Trabecular Surfaces of Female Subjects Aged 1 to 84  
740 Years. *Journal of Bone and Mineral Research* **31**, 347–357 (2016). 10.1002/jbmr.2696
- 741 51. Burr, D. B. Changes in bone matrix properties with aging. *Bone* **120**, 85–93 (2019).  
742 10.1016/j.bone.2018.10.010
- 743 52. Creecy, A. *et al.* The age-related decrease in material properties of BALB/c mouse long bones  
744 involves alterations to the extracellular matrix. *Bone* **130**, 115126 (2020).  
745 10.1016/j.bone.2019.115126
- 746 53. Cui, J., Shibata, Y., Zhu, T., Zhou, J. & Zhang, J. Osteocytes in bone aging: Advances, challenges,  
747 and future perspectives. *Ageing Research Reviews* **77**, (2022). 10.1016/j.arr.2022.101608
- 748 54. Ferretti, M., Muglia, M. A., Remaggi, F., Cane, V. & Palumbo, C. Histomorphometric study on  
749 the osteocyte lacuno-canalicular network in animals of different species. II. Parallel-fibered and  
750 lamellar bones. *Ital J Anat Embryol* **104**, 121–131 (1999).

- 751 55. Schemenz, V. *et al.* Heterogeneity of the osteocyte lacuno-canalicular network architecture and  
752 material characteristics across different tissue types in healing bone. *J Struct Biol* **212**, (2020).  
753 10.1016/j.jsb.2020.107616
- 754 56. Hernandez, C. J., Majeska, R. J. & Schaffler, M. B. Osteocyte density in woven bone. *Bone* **35**,  
755 1095–1099 (2004). 10.1016/j.bone.2004.07.002
- 756 57. Hasegawa, T. Ultrastructure and biological function of matrix vesicles in bone mineralization.  
757 *Histochemistry and Cell Biology* **149**, 289–304 (2018). 10.1007/s00418-018-1646-0
- 758 58. Golan, S., Elata, D. & Dinnar, U. Cortical Bone Periosteocytic Space Morphology Can Affect  
759 Osteocyte-Level Mass Flows and Shear Stresses. in *Engineering Systems Design and Analysis*  
760 **48364**, 77–84 (2008).
- 761 59. Rohrbach, D. *et al.* Spatial distribution of tissue level properties in a human femoral cortical bone.  
762 *J Biomech* **45**, 2264–2270 (2012). 10.1016/j.jbiomech.2012.06.003
- 763 60. Birkhold, A. I., Razi, H., Duda, G. N., Checa, S. & Willie, B. M. Tomography-Based  
764 Quantification of Regional Differences in Cortical Bone Surface Remodeling and Mechano-  
765 Response. *Calcif Tissue Int* **100**, 255–270 (2017). 10.1007/s00223-016-0217-4
- 766 61. Sun, Y. *et al.* Mechanical Stimulation on Mesenchymal Stem Cells and Surrounding  
767 Microenvironments in Bone Regeneration: Regulations and Applications. *Frontiers in Cell and*  
768 *Developmental Biology* **10**, (2022). 10.3389/fcell.2022.808303
- 769 62. Han, Y., Cowin, S. C., Schaffler, M. B. & Weinbaum, S. *Mechanotransduction and strain*  
770 *amplification in osteocyte cell processes*. *PNAS* **101**, (2004).
- 771 63. Rath Bonivtch, A., Bonewald, L. F. & Nicolella, D. P. Tissue strain amplification at the osteocyte  
772 lacuna: A microstructural finite element analysis. *J Biomech* **40**, 2199–2206 (2007).  
773 10.1016/j.jbiomech.2006.10.040
- 774 64. McCreddie, B. R., Hollister, S. J., Schaffler, M. B. & Goldstein, S. A. Osteocyte lacuna size and  
775 shape in women with and without osteoporotic fracture. *J Biomech* **37**, 563–572 (2004).  
776 10.1016/S0021-9290(03)00287-2
- 777 65. Belanger, L. R. Osteocytic Osteolysis. *Calcif Tissue Int* **12**, 1–12 (1969).
- 778 66. Dole, N. S. *et al.* Osteocyte-intrinsic TGF- $\beta$  signaling regulates bone quality through  
779 perilacunar/canalicular remodeling. *Cell Rep* **21**, 2585–2596 (2017).
- 780 67. Schurman, C. A., Verbruggen, S. W. & Alliston, T. Disrupted osteocyte connectivity and  
781 pericellular fluid flow in bone with aging and defective TGF-  $\beta$  signaling. 1–11 (2021).  
782 doi:10.1073/pnas.2023999118/-/DCSupplemental.Published 10.1073/pnas.2023999118/-  
783 /DCSupplemental.Published

- 784 68. Carter, Y., Thomas, C. D. L., Clement, J. G. & Cooper, D. M. L. Femoral osteocyte lacunar  
785 density, volume and morphology in women across the lifespan. *J Struct Biol* **183**, 519–526 (2013).  
786 10.1016/j.jsb.2013.07.004
- 787 69. Carter, Y. *et al.* Variation in osteocyte lacunar morphology and density in the human femur—a  
788 synchrotron radiation micro-CT study. *Bone* **52**, 126–132 (2013).
- 789 70. Bach-Gansmo, F. L. *et al.* Osteocyte lacunar properties and cortical microstructure in human iliac  
790 crest as a function of age and sex. *Bone* **91**, 11–19 (2016).
- 791 71. Buenzli, P. R. & Sims, N. A. Quantifying the osteocyte network in the human skeleton. *Bone* **75**,  
792 144–150 (2015). 10.1016/j.bone.2015.02.016
- 793 72. Dong, P. *et al.* 3D osteocyte lacunar morphometric properties and distributions in human femoral  
794 cortical bone using synchrotron radiation micro-CT images. *Bone* **60**, 172–185 (2014).  
795 10.1016/j.bone.2013.12.008
- 796 73. Varga, P. *et al.* Investigation of the three-dimensional orientation of mineralized collagen fibrils in  
797 human lamellar bone using synchrotron X-ray phase nano-tomography. *Acta Biomater* **9**, 8118–  
798 8127 (2013). 10.1016/j.actbio.2013.05.015
- 799 74. Hesse, B. *et al.* Canalicular network morphology is the major determinant of the spatial  
800 distribution of mass density in human bone tissue: Evidence by means of synchrotron radiation  
801 phase-contrast nano-CT. *Journal of Bone and Mineral Research* **30**, 346–356 (2015).  
802 10.1002/jbmr.2324
- 803 75. Matthews, M. M., Cook, E., Naguib, N., Wiesner, U. B. & Lewis, K. J. Intravital imaging of  
804 osteocyte integrin dynamics with locally injectable fluorescent nanoparticles. *Bone* **174**, (2023).  
805 10.1016/j.bone.2023.116830  
806